Development of stratified porous scaffolds based on polyesters as supports for indirect cell co-culture

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One of the main problems in the field of biomaterials and drug development is the use of animals in experimentation, which is an ethical issue that concerns all the society.[1] In this sense, tissue engineering is working to find alternatives. One of these alternatives is the development of *in vitro* models based on polymer supports for *in vitro* cell growth. These structures, moreover, could be used not only in drug testing or *in vitro* research to reduce the use of animals in experimentations, but also for tissue regeneration, simulating from simple tissues in which there is a single cell type, to more complex tissues from cell co-culture.[2]

Thus, a three-dimensional system with a stratified porous structure have been developed to allow both indirect cell co-culture and drug release assays (Figure 1). For this purpose, porous supports (scaffolds) have been obtained by means of the solvent-casting particle-leaching technique using salt as porogen, whose pore size allows cells to be housed in its interior, on which electrospun membranes have been arranged, forming a sandwich structure. These membranes form a structure of cross-linked fibers, leaving spaces between them that are much smaller than the cell size, so that they allow the passage of nutrients and molecules through them, but act as a barrier to the cells, preventing their migration to other areas of the three-dimensional system.[3]

Different polyesters were used to adjust the hydrophilicity, biodegradability, drug release kinetics and biological behavior, as desired. Moreover, fiber diameter was stablished at 1.8 μ m and membranes with and without curcumin as model drug were obtained by modifying the electrospinning parameters.[4] Curcumin was introduced by two methods: blend and coaxial electrospinning, so different delivery profiles were observed due to in blend electrospinning curcumin is placed in the whole fiber, while in coaxial electrospinning forms

the core.[5] For that reason, in coaxial electrospinning the release depends strongly on the degradation, that is higher for polylactic acid and poly(lactic-co-glycolic) than $poly(\epsilon)$ -caprolactone).

Because of the thickness limit of electrospinning, the 3D structure was obtained by using a sacrifice membrane. [6]

Finally, its use in indirect cell co-culture was tested by seeding fibroblast L929 in the scaffold, showing that scaffold allow cells to proliferate inside them, preventing an outside migration, so that indirect cell co-culture can be achieved by means of these structures.

References

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Figures



Figure 1. Scheme of the three-dimensional structure