

# Mastering Contrast Agents in a Single Structure for $T_1$ - $T_2$ Dual Magnetic Resonance Imaging

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**Introduction.** Signal Intensity (SI) in Magnetic resonance imaging (MRI) depends on longitudinal ( $T_1$ ) and transversal ( $T_2$ ) relaxivity times.<sup>1</sup> Unfortunately, the intrinsic contrast changes associated to a pathologic condition are often too limited for accurate diagnosis. Here, MRI contrast agents (CA) improve image resolution based on their selective accumulation in the Region Of Interest.<sup>2</sup> These CAs are classified as positive ( $T_1$ -weighted) or negative ( $T_2$ -weighted) image contrast promoters. The acquisition of MRI weighted in  $T_1$  and  $T_2$  could improve the safety of diagnosis.<sup>3</sup> In this context, it has been reported that Prussian Blue (PB) derivatives with general molecular formula  $K_xGd_{1-x}(H_2O)_n[Fe(CN)_6]$  and nanosized crystallites present high performance as dual  $T_1$ - $T_2$  CAs.<sup>4</sup> Unfortunately, their clinical use is precluded by the partial solubility in physiological medium. In this work, to protect  $Gd(H_2O)_4[Fe(CN)_6]$  nanoparticles we have coated them with a thin amorphous silica shell by polymerizing the silicate at neutral pH, obtaining an stable CA for *in vivo* MRI.

**Results and Discussion.** The combination of Gd and Fe magnetic centers closely packed at the same crystalline structure leads to a magnetic synergistic effect, which results in an outstanding improve-

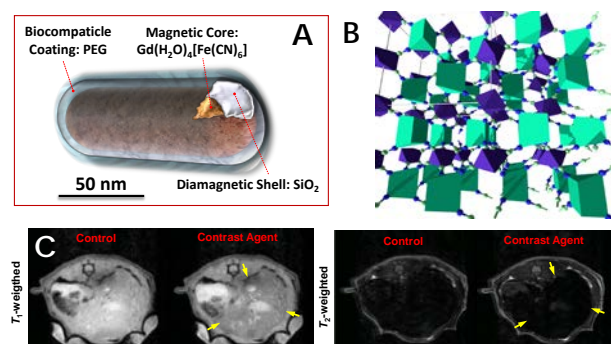
ment of longitudinal relaxivity with regards to soluble  $Gd^{3+}$  chelates, whilst keeping the high transversal relaxivity inherent to iron oxide nanoparticles. This CA improves positive and negative contrast in  $T_1$ - and  $T_2$ -weighted MR images, both in *in vitro* and *in vivo* systems. Furthermore, this novel hybrid presents a high biosafety profile and has strong ability to incorporate organic molecules on surface, displaying great potential for further clinical application.

**Conclusion.** With regards other proposed  $T_1$ - $T_2$  dual mode CAs, these nanoparticles present very homogeneous composition and constant Gd:Fe atomic ratio, providing reproducible quality in MRI signal.

## References

- [1] R. Zakaria, K. Das, M. Bhojak, M. Radon, C. Walker and M. D. Jenkinson, *Cancer Imaging*, 14 (2014) 8.
- [2] W. Cheng, Y. Ping, Y. Zhang, K. H. Chuang and Y. Liu, *J. Healthc. Eng.*, 4 (2013) 23.
- [3] Z. Zhou, R. Bai, J. Munasinghe, Z. Shen, L. Nie and X. Chen, *ACS Nano*, 11 (2017) 5227.
- [4] V. S. Perera, L. D. Yang, J. Hao, G. Chen, B. O. Erokwu, C. A. Flask, P. Y. Zavalij, J. P. Basilion and S. D. Huang, *Langmuir*, 30 (2014) 12018.

## Figures



**Figure 1:** (A) Artistic representation of Gd-PB nanoparticle protected with a silica shell. (B) Network topology of  $Gd(H_2O)_4[Fe(CN)_6]$ . (C) *In vivo* coronal  $T_1$ - and  $T_2$ -weighted images acquired from a male Sprague-Dawley rat at 7 T magnetic field.