



# **3D-Graphene based Pressure and Strain Sensor**

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## Abstract

We demonstrate a broad range and fast response pressure and strain sensor using a flexible and conductive 3D graphene structure. The sensor can detect small pressures/strains and various biological signals from the movement of human skin. The active element of sensor consists of a 3D graphene nanoporous framework made of graphene sheets separated with air-filled pores. A simple hydrothermal technique followed by freeze-drying and high-temperature thermal annealing is used for the synthesis of 3D graphene aerogel. The resulting graphene aerogel is highly elastic and the contact resistance between aerogel and rigid metal electrode is highly sensitive to applied stimuli. The extraordinary sensitivity of the contact resistance permits the detection down to a few micrometers by a small change of the sample size. In addition, the elastic nature of graphene aerogel provides high responsivity to the sensor, allowing detecting fast actions down to a few milliseconds and temperature independent. We show that the 3D graphene-based sensors can be used as wearable electronic sensors for diverse kinds of biological motion detection, human-machine interface and soft robotics applications.

Figure 1: Actual pictures of the materials obtained after every step of

synthesizing 3D graphene aerogels (scale bar: 1 cm).







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## **Objectives**

- For human-machine interface and skin monitoring devices, the pliable nature of the skin requires sensors with a wide dynamic range and high sensitivity 0.2-500 kPa.
- There is no electromechanical sensor that would cover such a high range in tensile and compression.
- The traditional piezoresistive sensors based on bulk piezo resistivity variation have a limited range of operation, and are not different measuring suitable for physiological signals.
- development novel sensing The of mechanisms and materials that can emulate strain and pressure-sensing properties of natural skin.

#### Experimental Synthesis of 3D graphene **Characterization of Graphene Aerogels** ii iii C1s 01s Freeze drying (- 70 °C) (a.u.) (a.u.) (a.u.) Annealing (1300 °C) Hydrothermal **(a)** ₹ Intensity Intensity Intens **(b) (b)** Graphene GO homogeneous solution **RGO-Hydrogel** (2mg GO per ml of water) Aerogel 284 288 535 286 282 290 530 540 1100 525

B.E. (eV)

2D (a.u.) **(a)** Intensity (c) 2200 2750 20 30 1650 40 Raman shift (cm<sup>-1</sup>) 2θ (Deg.)

iv

002)

**(a)** 

**(b)** 

(c)

50

Figure 2: (i-ii) XPS spectra of C 1s and O 1s of graphene aerogel (a) before and (b) after annealing. (iii) Raman spectra and (iv) X-ray diffractograms of the graphene aerogel (a) before annealing (dark yellow) (b) after annealing (magenta) and (c) 70% compressed sample (blue).

B.E. (eV)

# **Doculte and Discussion**

Sensor Characterization	Sensing mechanism		<b>Dynamic Response and Sensor Performance</b>
Compressive			i ii



Figure 3: Electrical response of GA strain sensors under compression and tension. (i and iv) Current  $(\Delta I/I_0)$  response and (ii and v) relative resistance change  $(\Delta R/R_0)$  of GA sensors with applied compressive and tensile stress, respectively. (iii and vi) The current response of the GA sensors as a function of compressive and tensile stress, showing two sensitivity regimes. The slope of the curves was used to calculate the gauge factor (GF =  $(\Delta R/R_0)/\epsilon N$ ) and sensitivity (S =  $(\Delta I/I_0)/\Delta P$ ) of the sensors.

Figure 4: (i-ii) Schematics of experimental set-ups for contact resistance measurements in two-probe and four-probe configurations. (iii) Measured resistance of the device under stress using the 2-probe and 4-probe methods. (iv) Relationship between resistance and pressure in a  $\log(R)$  and  $\log(P)$  scale using the 2-probe method.

Figure 5: (i) The instant voltage response of a GA sensor demonstrating the response time of 0.52 ms. (ii) An example of a GA sensor detecting ultralow force (iii) the reproducibility of the pressure sensor after 5,000 loading-unloading cycles. (iv) Comparison of the response time and maximum pressure limit of the GA sensors with different strain sensors based on GA and other materials.

#### **Applications** Human Pulse measurement **Tactile sensing: Weight measurement Finger movement measurement** iii iv bodily actions. 1.5 1.6 1000 bottle 2 Measured weight 0.45 85° (515 a)

# Conclusion

- The sensors have demonstrated a remarkably broad working range both in tensile (0-0.55 MPa) and compressive (0-1.18 MPa) stress, which enables them to cover the whole range of human
- The sensors have also shown high sensitivity with a gauge factor in the range of 0.38-11.6 in the



Figure 6: Tactile sensing using a 3D GA sensor. (i) The current ( $\Delta I/I_0$ ) response of a GA sensor attached above the artery of the wrist detecting a pulse as a function of time. (ii) The current response of a GA sensor attached to an index finger when grasping objects of variable weight. The inset shows an optical image of a magnet lifting using the thumb and index fingers. (iii) The real weight and measured weight of different picked objects by the sensor. (iv) The current signals corresponding to finger-bending motions. The inset shows optical images of finger bending with the attached sensor.

## compressive mode and 0.6-3.4 in the tensile mode, respectively.

- The sensors provide long-term stability over 5000 compressing-relaxing cycles and a fast response time of  $5.2 \times 10^{-4}$  s. .
- We have proposed that the observed piezoresistive sensing mechanism is originating from the variation of the contact resistance of the interface between the porous graphene aerogel and metal contacts.
- The reported graphene aerogel sensors have a high potential for applications in biomedicine, wearable electronics, and tactile robotic applications.

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